

# Classification of EEG Signal for Epileptic Seizure Detection using EMD and ELM

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**Abstract**—This paper proposes the classification of EEG signal for epilepsy diagnosis. Epilepsy is a neurological disorder which occurs due to synchronous neuronal activity in brain. Empirical Mode Decomposition (EMD), Extreme Learning Machine (ELM) are the techniques delivered in the proposed method. Input EEG signal, which is available in online as Bonn Database is decomposed into five Intrinsic Mode Functions (IMFs) using EMD. Higher Order Statistical moments such as Variance, Skewness and Kurtosis are drawn out as features from the decomposed signals. Extreme Learning Machine is used as a classifier to classify the EEG signals with the taken features, under various categories that include healthy and ictal, interictal and ictal, Non seizure and seizure, healthy, interictal and ictal. The proposed method gives 100% accuracy, 100% sensitivity in discriminating interictal and ictal, non seizure and seizure, healthy and ictal, healthy, interictal and ictal, 100% specificity in classifying healthy and ictal, interictal and ictal and 100% and 99% accuracy in case of discriminating interictal and ictal, non seizure and seizure.

**Index Terms**—Electroencephalogram (EEG), Empirical Mode Decomposition (EMD), Extreme Learning Machine (ELM), Feature Extraction, seizure detection.

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## 1 INTRODUCTION

Epilepsy is a disorder which happens due to unusual discharges in brain. The intense electrical activity causes a temporary disruption to normal brain making the brain's messages get mixed up. This results in recurrent seizures. About 60 million people are suffered with epilepsy in the world. Epileptic seizures fall into two types namely Partial seizures and Generalized seizures. Partial seizures impact only a portion of the brain which leads to temporal paralysis and generalized seizures involve electrical discharges that occur all over the brain which cause loss of consciousness.

Electroencephalogram (EEG), being a non-invasive tool evaluates the patient with epilepsy. It examines the brain patterns and assists in epilepsy diagnosis, if any unusual activity takes place in the brain. Extracranial EEG measurements are obtained by keeping electrodes on the scalp whereas Intracranial EEG (iEEG) recordings are examined by keeping electrodes on the cortex of the brain or deep within the structure of the brain. For a normal brain activity, the firing of neuron occurs about 80 times per second and neurons fire about 500 times per second for an epileptic brain activity.

Various approaches have been integrated for the seizure detection. Shafiul Alam et al. proposed seizure detection using Artificial Neural Network

(ANN). Empirical Mode Decomposition is used for decomposition purpose [1]. Shufang Li et al. used EMD to extract coefficient of variation and fluctuation index as features. Support Vector Machine (SVM) classifier is utilized for the classification of interictal and ictal subjects [2]. Complexity based features are taken using Wavelet Transform and the features are selected using Genetic Algorithm. Extreme Learning Machine is used as the classifier for recognizing the epileptic activities. The method proposed by Yuedong Song et al. gives less accuracy without the use of Genetic Algorithm [3]. Bandwidth features namely Amplitude Modulation Bandwidth and Frequency Modulation Bandwidth is computed using EMD techniques and these features were fed to the Least Square Support Vector Machine (LS-SVM) for classification purpose [4]. Nandish et al. used Average method and Max-Min method for taking the features. Among the two methods Max-min with Neural Network gave better accuracy [6]. Fuzzy classifier could be able to discriminate healthy, interictal and ictal subjects with good accuracy by the usage of entropy features [7]. Multiwavelet Transform along with ANN technique had been used by Ling Guo et al. Entropy based features are extracted for classifying healthy and epileptic subjects. Computation cost increases due to the excessive number of features [11]. EEG signal is analysed with time-frequency methods and Artificial

Neural Network (ANN)[16]. Usage of ANN makes high computational complexity and takes huge training time.

EMD delivered by Huang is widely adaptable to non-stationary and nonlinear signals. It is used in the case of reducing noise and providing information. In this paper, classification of EEG signal for epileptic seizure detection is done with EMD and ELM. Variance, Skewness and Kurtosis are taken as features, which describes the shape of EEG signals. The features are then trained and tested using ELM classifier to discriminate healthy, interictal and ictal subjects under different cases. ELM classifier requires no iterative tuning and classifies signal with good accuracy.

## 2 METHODOLOGY

This section has three steps.

- i) Decomposition of input signal
- ii) Feature Extraction
- iii) Classification of EEG signal



Fig. 1. Block diagram of Seizure detection using EMD- ELM

### 2.1 DatabaseDescription

Bonn Database [18] from the Department of Epileptology is used. The dataset is possessed with five sets namely Z, O, N, F, S. The dataset Z and O have EEG recordings that were obtained from healthy subjects with their eyes opened and closed respectively. The measurements for the set Z and O were carried out using extracranial electrodes. The dataset N, F, S have recordings from epileptic patients. Sets F and N have EEG measurements that were observed, intracranially during seizure free interval, from epileptogenic zone and from hippocampal formation of opposite hemisphere of the brain. The dataset S has ictal EEG recordings from the epileptogenic zone. The 100 single channel EEG signals from each person are recorded in 23.6s with the sampling rate of 173.6Hz.

### 2.2 EmpiricalModeDecomposition

An adaptive, nonlinear technique referred as Empirical Mode Decomposition (EMD) fragments the nonstationary signal into Amplitude-Frequency modulated components namely Intrinsic Mode Function (IMF).

The block diagram of seizure detection using EMD with ELM is given in Fig.1. The steps involved in EMD Algorithm is given below

- i) Take an input signal  $s$  and consider it to be  $s=h, n=0$
- ii) Local maxima and Local minima of input signals are found

- iii) Upper envelope ( $e_{max}$ ) and lower envelope ( $e_{min}$ ) are found by connecting the local maximum and local minimum respectively, through cubic spline function
- iv) Mean of upper envelope and lower envelope are determined

$$m = (e_{max} + e_{min}) / 2 \quad (1)$$

- v) The value of mean should be subtracted from the input signal

$$H = h - m \quad (2)$$

- vi) Check whether the stopping criterion ( $\alpha$ ) lies in the range 0.2-0.3, in the calculation of standard deviation given in (3). If the condition is satisfied then take  $imf_n = H, n=n+1$  and go to the step vii, else consider the input signal  $s$  as  $H$  i.e.  $s=H$  and repeat the process from i to vi

$$sd = \frac{\sum |H-h|^2}{\sum h^2} < \alpha \quad (3)$$

- vii) Calculate residue signal  $r = h - imf_n$ , if  $r$  is a function of monotonicity end the process else consider  $s=r$  and repeat from (i)

Empirical mode decomposition is more adaptable to nonlinear and nonstationary signals. The frequency component decreases, as the number of intrinsic mode function level increases. The information does not get lost when the frequency decreases. Flow chart of EMD algorithm is given in Fig.2.

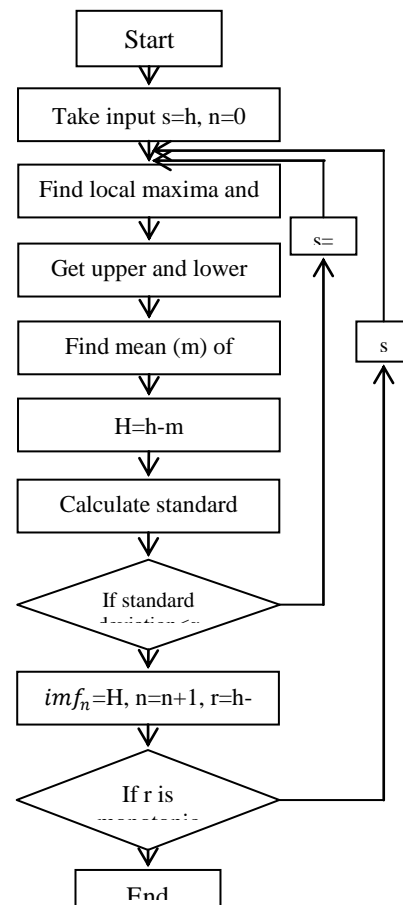


Fig. 2. EMD Algorithm

The original signal(s) can be regained by adding IMFs level and residue signal(r) that have the lowest frequency. The representation of original signal is given by (4)

$$s = \sum_{n=1}^N imf_n + r \quad (4)$$

### 2.3 Feature Extraction

Variance, Skewness and Kurtosis are taken as features from the decomposed signals of EMD. Variance ( $\sigma^2$ ), Skewness (sk) and Kurtosis (ku) are given by

$$\sigma^2 = \frac{1}{N} \sum_{i=1}^N (x_i - \mu)^2 \quad (5)$$

$$Sk = \frac{1}{N} \sum_{i=1}^N \left( \frac{x_i - \mu}{\sigma} \right)^3 \quad (6)$$

$$Ku = \frac{1}{N} \sum_{i=1}^N \left( \frac{x_i - \mu}{\sigma} \right)^4 \quad (7)$$

where the mean ( $\mu$ ) is  $\mu = \frac{1}{N} \sum_{i=1}^N x_i$ , N is the length of imf (N=1024),  $x_i$  is the imf of signal for ith sample and

$$\text{standard deviation } (\sigma) \text{ is } \sigma = \sqrt{\frac{1}{N} \sum_{i=1}^N (x_i - \mu)^2}$$

Variance, Skewness and Kurtosis describes the dispersion, asymmetry and peakness of the dataset.

### 2.4 Extreme Learning Machine

Extreme Learning Machine makes use of Single hidden layer feed forward neural network (SLFN). Architecture of ELM is given in Fig.3. Single hidden layer feed forward neural network (SLFN) possessing L-hidden node with additive and Radial Basis Function (RBF) is given by

$$\beta_j g(w_j, b_j, x_i) = o_j \quad (8)$$

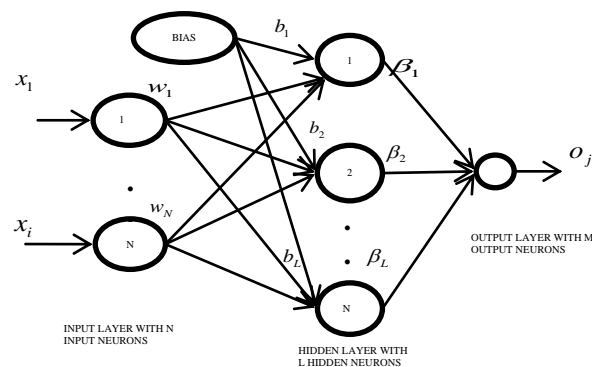


Fig. 3. ELM Architecture

The activation function for additive hidden node and Radial Basis Function hidden node is given (9) and (10)

$$g(w_j, b_j, x_i) = g(w_j \cdot x_i + b_j) \quad (9)$$

$$g(w_j, b_j, x_i) = g(b_j \|x_i - w_j\|) \quad (10)$$

$w_j$  is the weight vector connecting the input layer to the jth hidden node and  $b_j$  is the bias of the jth hidden node. For N samples with L hidden nodes that has zero error can be given as  $T = \beta H$  where  $\beta$  is the weight between hidden and output layer and T is the target. Unipolar sigmoidal activation function is given by

$$G(w_j, x_i, b_j) = \frac{1}{1 + e^{-(w_j \cdot x_i + b_j) \cdot \lambda}} \quad (11)$$

where  $\lambda$  is the learning parameter that ranges between 0 to 1.

ELM is carried out three steps that require no tuning. It involves

- i) Assigning randomly input weights (w) and bias (b)
- ii) Calculating the hidden layer output matrix H
- iii) Determining the output weights  $\beta^{\wedge} = H^{-1}T$  where  $H^{-1}$  is the Moore Penrose generalized inverse of H. The steps are summarized and given in Fig.4.

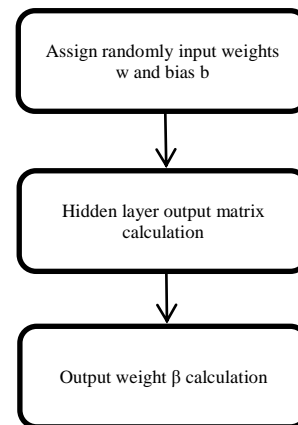


Fig. 4. Steps for ELM

### 3 PERFORMANCE MEASURES

The performance analysis is carried out by finding Sensitivity, Specificity and Accuracy.

$$\text{Sensitivity} = TP / (TP + FN) \quad (12)$$

$$\text{Specificity} = TN / (TN + FP) \quad (13)$$

$$\text{Accuracy} = (TP + TN) / (TP + FN + TN + FP) \quad (14)$$

Where TP, FN, TN, FP represents True Positive, False Negative, True Negative, False Positive respectively.

### 4 RESULTS AND DISCUSSIONS

Feature extraction and classification of EEG signal is presented using Empirical Mode Decomposition (EMD) with Extreme Learning Machine (ELM) classifier. Bonn dataset being sampled at 173.6 Hz is band limited to 86.8 Hz. When decomposition is analysed with EMD, the frequency ranges of first five IMF are given: IMF1 (0–44 Hz), IMF2 (0–30

Hz), IMF3 (0–20Hz), IMF4 (0–9Hz), IMF5 (0–7 Hz). The frequency range gets decreased to the range 0-3 Hz for the 6<sup>th</sup> IMF.

The epileptic EEG signal deals with the frequency range of 3-29 Hz. So First Five IMF of the signal is used when the decomposition is carried out using EMD. Fig. 5, Fig. 6, Fig.7 shows healthy EEG signal with five imfs, interictal EEG signal with five imfs, ictal EEG signal with five imfs respectively. The amplitude and frequency modulated oscillatory patterns are well noticed from the generated imfs.

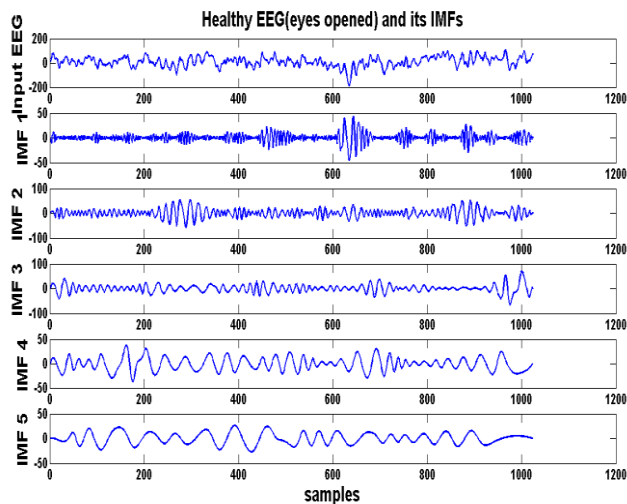


Fig. 5. Healthy EEG (eyes opened) and its five imfs using EMD

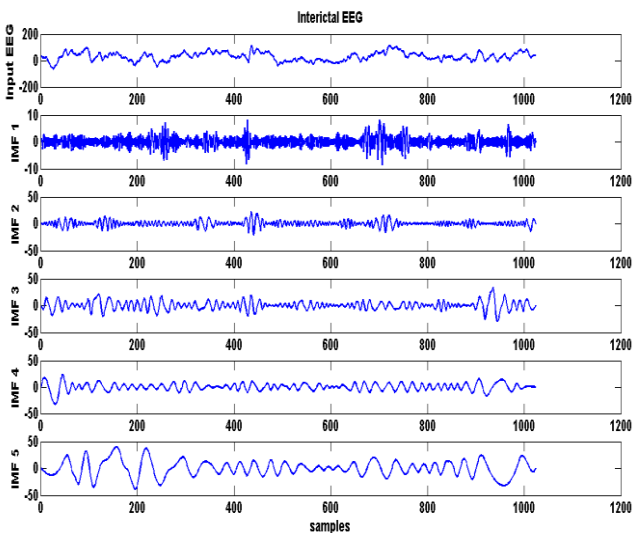


Fig. 6. Interictal EEG and its five imfs using EMD

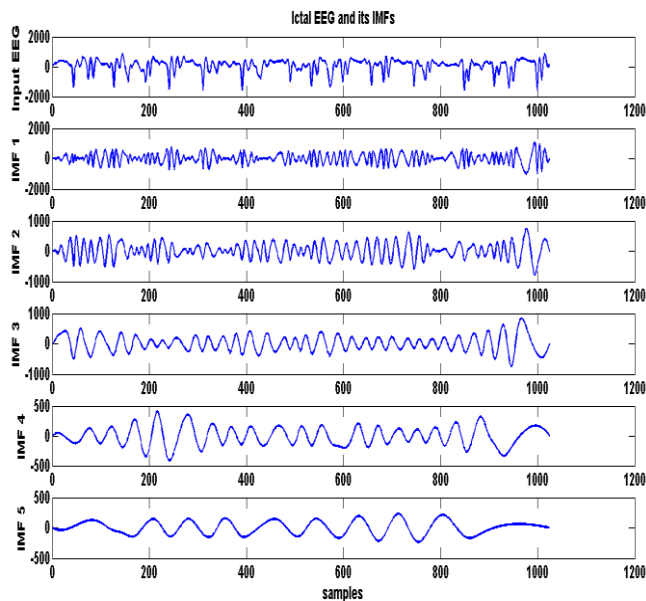


Fig. 7. Ictal EEG and its five imfs using EMD

The extracted features namely variance, skewness and kurtosis are shown in histogram to define the shape of healthy, interictal and ictal EEG signals. Histogram of healthy, interictal and ictal EEG signals are shown in Fig. 8. (a), Fig. 8. (b), Fig. 8. (c) respectively. Mean value of ictal EEG signal is high when compared to interictal and healthy EEG signals. From the histogram diagram, it is seen that the EEG signal's shape differs with the seizure occurrence and nonseizure occurrence

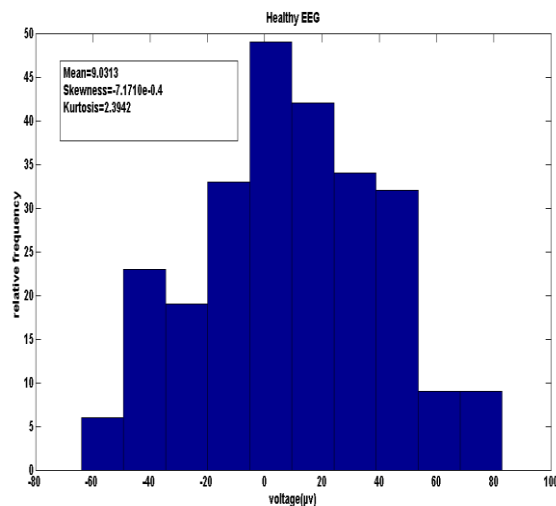


Fig. 8. (a) Histogram of healthy EEG

Fig. 9. (a), Fig. 9. (b), Fig. 9. (c) depicts the histogram of IMF2 of healthy, interictal and ictal EEG signals respectively.

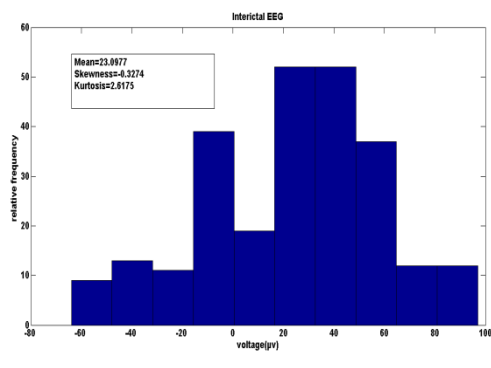


Fig. 8. (b) Histogram of interictal EEG

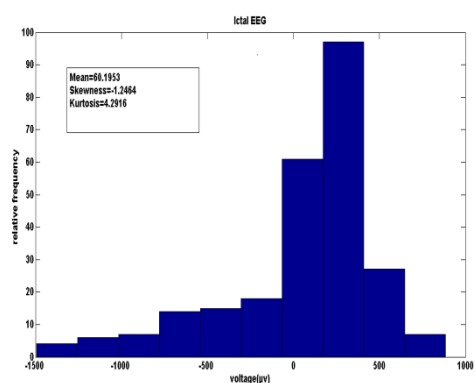


Fig. 8. (c) Histogram of ictal EEG

Classification is done under different case using Extreme Learning with unipolar sigmoidal activation function. Table-I gives the performance analysis of EEG signal classification using single imfs. Classifiers namely C-1, C-2, C-3, C-3 are formed using three features from the five single IMFs. In Case I, sets Z, O, N and F together forms the non-seizure class and sets S form the seizure class. 100% specificity with 99% accuracy is got in C-3 where 100% sensitivity is obtained in C-1 and C-2 while discriminating non seizure from seizure ones. Case-II delivers the classification of EEG signal for healthy subjects (Z) and ictal subjects (S) with accuracy of 96.88%, 100% sensitivity and 94% specificity. Perfect classification is achieved in Case-III which depicts the discrimination of interictal and ictal EEG signals. 100% sensitivity, 100% specificity and 100% accuracy is accomplished in this case.

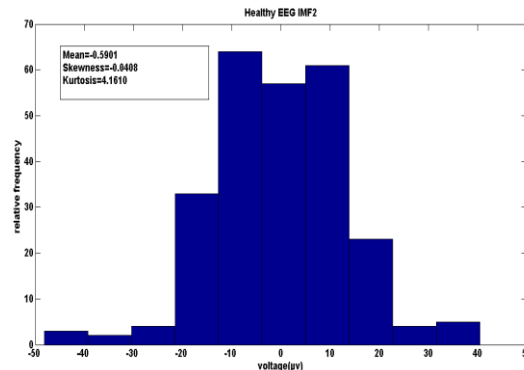


Fig. 9. (a) Histogram of IMF 2 of healthy EEG

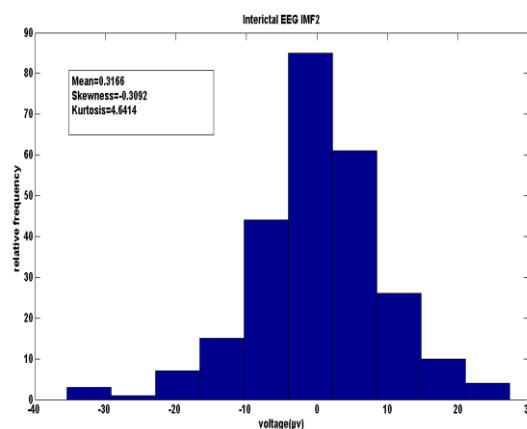


Fig. 9. (b) Histogram of IMF 2 of interictal EEG

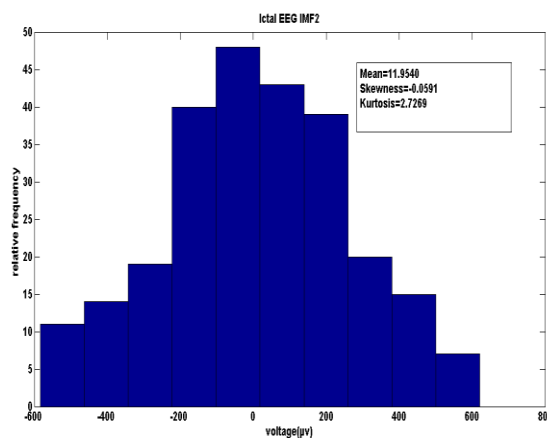


Fig. 9. (c) Histogram of IMF 2 of ictal EEG

Case-IV deals in distinguishing healthy, interictal and ictal class. Accuracy of 98% is got in discriminating ictal from interictal and healthy subjects. In Case-V, sets Z and O are grouped to healthy subjects, sets N and F are tagged to interictal subjects and set E forms the ictal class. 100% sensitivity, 100% specificity and 100% accuracy is obtained in distinguishing ictal class from healthy and interictal class. Table-II exhibits the classification performance of EEG signal using multiple IMFs. Features from five IMFs are combined and they are given to the classifier C-6.

**TABLE 1**  
**CLASSIFICATION PERFORMANCE USING SINGLE**  
**IMFs**

CLASSIFIERS		C-1	C-2	C-3	C-4	C-5
Case I (Z,O,N, F),S	Sensitivity	<b>100</b>	<b>100</b>	<b>93.33</b>	<b>93.3</b>	<b>100</b>
	Specificity	82.9	<b>97.14</b>	<b>100</b>	<b>94.29</b>	81.86
	Accuracy	85.88	<b>97.65</b>	<b>99</b>	<b>94.12</b>	84.52
Case II Z,S	Sensitivity	<b>93.33</b>	<b>100</b>	<b>93.33</b>	<b>93.33</b>	<b>100</b>
	Specificity	<b>100</b>	<b>94.12</b>	<b>100</b>	82.35	70.59
	Accuracy	<b>96.88</b>	<b>96.88</b>	<b>96.88</b>	87.50	84.38
Case III N,S	Sensitivity	<b>100</b>	<b>100</b>	<b>100</b>	<b>100</b>	<b>100</b>
	Specificity	<b>100</b>	82.35	88.24	52.94	82.35
	Accuracy	<b>100</b>	<b>90.6</b>	<b>93.75</b>	75.00	<b>90.63</b>
Case IV O,F,S	Sensitivity(O)	<b>97</b>	87.88	81.82	<b>100</b>	<b>100</b>
	Specificity(O)	80	47.06	72.22	66.67	48
	Accuracy(O)	<b>91.67</b>	74	79	88.24	78.43
	Sensitivity(F)	<b>94.44</b>	84.85	61.11	83.33	44.64
	Specificity(F)	<b>90</b>	76.47	78.79	78.79	<b>90.91</b>
	Accuracy(F)	<b>92.11</b>	82	72	80.39	74.51
	Sensitivity(S)	<b>100</b>	<b>100</b>	86.67	86.67	<b>100</b>
	Specificity(S)	<b>97.22</b>	82.86	<b>97.22</b>	88.89	50
	Accuracy(S)	<b>98.04</b>	88	<b>94</b>	88.24	64.71
Case V (Z,O), (N,F),S	Sensitivity(ZO)	88	70	70	80	<b>92</b>
	Specificity(ZO)	51.43	60	85.71	35	25
	Accuracy(ZO)	73	65	76.19	61.18	63.10
	Sensitivity(NF)	84.62	60	57.14	53	40
	Specificity(NF)	63	84	<b>90</b>	55.10	76
	Accuracy(NF)	73	74.12	76.19	54.12	61.
	Sensitivity(S)	80	<b>100</b>	<b>100</b>	<b>100</b>	<b>100</b>
	Specificity(S)	<b>95.71</b>	88.57	<b>100</b>	88.73	53.62
	Accuracy(S)	<b>93</b>	<b>90.59</b>	<b>100</b>	<b>90.59</b>	62

**TABLE 2**  
**CLASSIFICATION PERFORMANCE USING**  
**MULTIPLE IMFs**

CLASSIFIER		C-6
Case I (Z,O,N,F),S	Sensitivity	88.71
	Specificity	34.71
	Accuracy	74.12
Case II Z,S	Sensitivity	80
	Specificity	<b>100</b>
	Accuracy	90.63
Case III N,S	Sensitivity	60
	Specificity	52.94
	Accuracy	57
Case IV O,F,S	Sensitivity(O)	61.76
	Specificity(O)	39
	Accuracy(O)	54
	Sensitivity(F)	63.16
	Specificity(F)	73
	Accuracy(F)	69.23
	Sensitivity(S)	20
	Specificity(S)	75.68
Case V (Z,O),(N,F),S	Accuracy(S)	58
	Sensitivity(ZO)	82
	Specificity(ZO)	88.57
	Accuracy(ZO)	84
	Sensitivity(NF)	65.71
	Specificity(NF)	<b>96</b>
	Accuracy(NF)	83.53
	Sensitivity(S)	80
Specificity(S)	88.5	
Accuracy(S)	87	

From the Table-I and Table-II, it is expressed that classification using single IMF gives good performance when compared to multiple IMF in most of the cases. Three features are taken when using with single IMF whereas fifteen features are used when dealing with multiple IMFs. The computational time gets reduced when performing with single IMF.

## 5 CONCLUSION

In this paper, classification of EEG signal for seizure detection under various cases that includes healthy and ictal, interictal and ictal, non seizure and seizure, healthy, interictal an ictal is proposed. EMD is applied to decompose the input signal into five IMFs. Higher order statistical features like variance, skewness and kurtosis are extracted from the decomposed signals to distinguish healthy, interictal and ictal subjects. The taken features are trained and tested using the ELM classifier. It has been exhibited that the proposed method shows 100% sensitivity, 100% specificity and 100% accuracy in most of the cases when discriminating with single IMF rather than multiple IMFs. Future enhancement can be done by including the case of classifying the EEG signal into sets Z, O, N, F, and S for epilepsy detection.

## REFERENCES

- [1] S.M. Shafiul Alam and M.I.H. Bhuiyan, "Detection of Seizure and Epilepsy Using Higher Order Statistics in the EMD Domain", *IEEE Journal of Biomedical and Health Informatics*, Vol.17, No.2, pp. 312-318, March 2013.
- [2] Shufang Li, Weidong Zhou and Dongmei Cai, "Feature Extraction and Recognition of Ictal EEG Using EMD and SVM", *Computers in Biology and Medicine*, Vol. 43, pp. 807-816, April 2013.
- [3] Yuedong Song, Jiayang Zhang, "Automatic recognition of epileptic EEG patterns via Extreme Learning Machine and multiresolution feature extraction", *Expert Systems with Applications*, vol.40, pp. 5477-5489, 2013.
- [4] Varun Bajaj and Ram Bilas Pachori, "Classification of Seizure and Nonseizure EEG Signals using Empirical Mode Decomposition", *IEEE Transactions on Information Technology in Biomedicine*, Vol.16, No.6, pp. 1135-1142, Nov. 2012.
- [5] S. M. Shafiul Alam, M. I. H. Bhuiyan, Aurangozeb, and Syed Tarek Shahriar, "EEG Signal Discrimination using Non-linear Dynamics in the EMD Domain", *International Journal of Computer and Electrical Engineering*, Vol.4, No.3, pp. 326-330, 2012.
- [6] M. Nandish, Stafford Michahial, P. HemanthKumar, "Feature Extraction and Classification of EEG Signal Using Neural Network Based Techniques", *International Journal of Engineering and Innovative Technology (IJEIT)*, Vol.2, No. 4, Oct.2012.

- [7] U. Rajendra Acharya, Filippo Molinari, S. Vinitha Sree, Subhagata Chattopadhyay, Kwan-Hoong Ng, Jasjit S. Surig, "Automated diagnosis of epileptic EEG using entropies", *Biomedical Signal Processing and Control, Elsevier*, vol.7, No. 4, pp.401–408, July 2012.
- [8] J. Siva Prakash, "Extreme Learning Machines - A Review and State-of-the-art", *International Journal of Wisdom based Computing*, Vol.1, No. 1, Apr.2011.
- [9] Tomasz M. Rutkowski, Danilo P. Mandic, Andrzej Cichocki, Andrzej W. Przybyszewski, "EMD Approach to Multichannel EEG Data — The Amplitude and Phase Components Clustering Analysis", *Journal of Circuits, Systems, and Computers*, Vol.19, No.1, pp. 215-229, 2010
- [10] Ali Shoeb, John Guttag, "Application of Machine Learning To Epileptic Seizure Detection", Appearing in Proceedings of the 27th International Conference on Machine Learning, Haifa, Israel, 2010.
- [11] Ling Guo, Daniel Rivero, Alejandro Pazos, "Epileptic seizure detection using multiwavelet transform based approximate entropy and artificial neural networks" *Journal of Neuroscience Methods*, vol. 193, No. 1, pp.156-63, Oct. 2010.
- [12] Guang-Bin Huang, Xiaojian Ding, Hongming Zhou, "Optimization method based extreme learning machine for classification", *Neurocomputing, Elsevier*, Vol.74, No. 1-3, pp. 155-163, Dec. 2010.
- [13] Jean-Claude Nunes, Eric Del Echelle, "Empirical Mode Decomposition: Applications on Signal and Image Processing", *Advances in Data Analysis*, Vol.1, No.1, Jan. 2009.
- [14] Alexandros T. Tzallas, Markos G. Tsipouras, and Dimitrios I. Fotiadis, "Epileptic Seizure Detection in EEGs Using Time-Frequency Analysis", *IEEE Transactions on Information Technology in Biomedicine*, Vol.13, No.5, pp.703-10, Sep. 2009.
- [15] Ram Bilas Pachori, "Discrimination between Ictal and Seizure-Free EEG Signals using Empirical Mode Decomposition", *Communication Research Centre*, Dec. 2008.
- [16] A.T. Tzallas, M. G. Tsipouras, D.I. Fotiadis, "Automatic Seizure Detection Based on Time-Frequency Analysis and Artificial Neural Networks", *Computational Intelligence and Neuroscience*, Dec. 2007, doi:10.1155/2007/80510
- [17] PariJahankhani, VassilisKodogiannis and Kenneth Revett, "EEG Signal Classification Using Wavelet Feature Extraction and Neural Networks", *IEEE John Vincent Atanasoff 2006 International Symposium on Modern Computing*, pp. 120-124, Oct. 2006.
- [18] Ralph G. Andrzejak, Klaus Lehnertz, Christoph Rieke, Peter David, Christian E. Elger, "Indications of nonlinear deterministic and finite-dimensional structures in time series of brain electrical activity: Dependence on recording region and brain state", *Physical Review E*, Vol.64, No.6, Nov. 2001.